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Noise Assumptions in Complex-Valued SENSE MR Image Reconstruction

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Noise Assumptions in Complex-Valued SENSE MR Image Reconstruction

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OUTLINE

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Motivation

In MRI k-space for images is not measured instantaneously.

In parallel imaging, sub-sampled k-space points are measured in parallel and combined to form a single image.

Image and volume measurement time is decreased at the expense of increased image reconstruction difficulty and time.

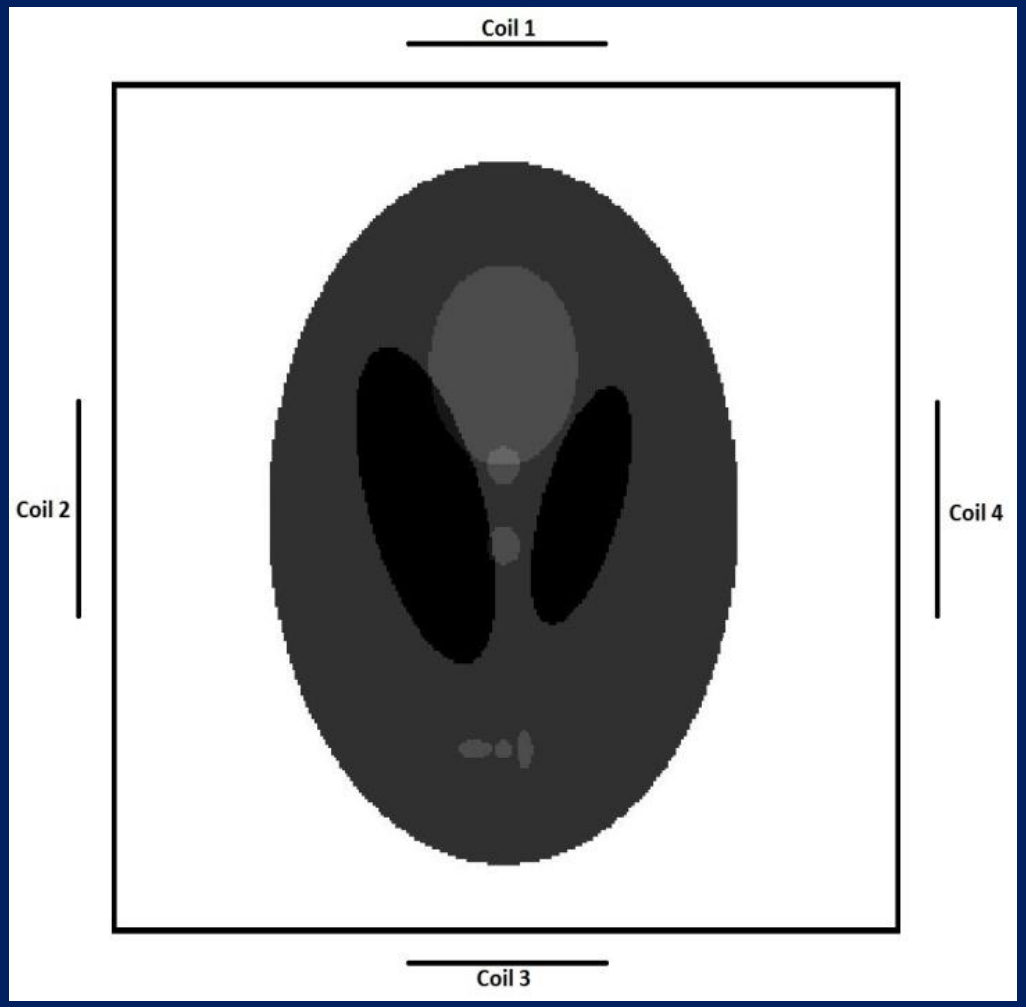
The SENSE parallel imaging reconstruction technique utilizes a complex-valued least squares estimation process.

However, in SENSE the covariance is not properly modeled.

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.

Background

In parallel imaging there is more than one receive coil.



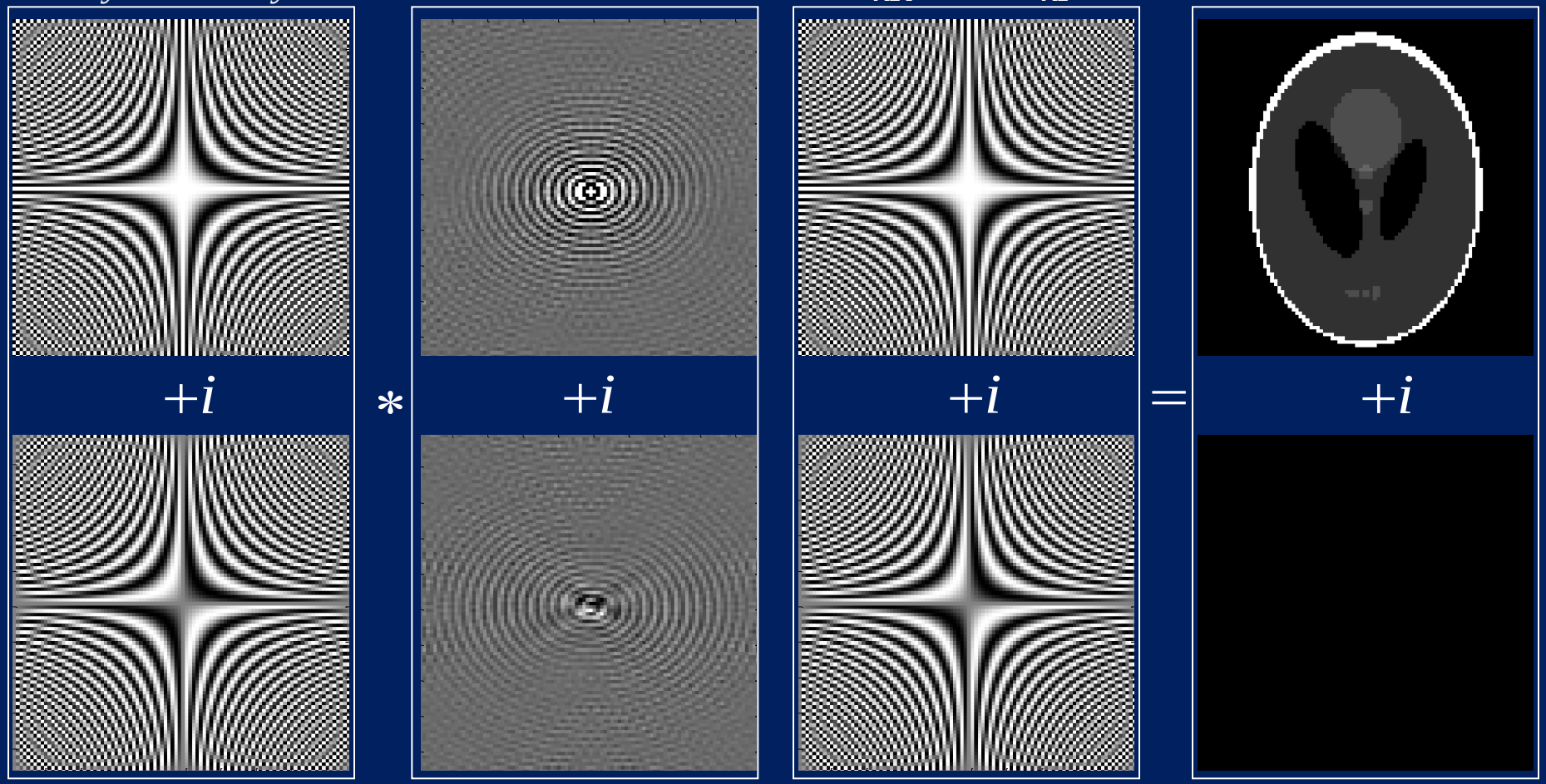
Each coil measures a k-space array that is reconstructed into an aliased image then combined to form a single unaliased image.

Bruce and Rowe: In progress.

Background

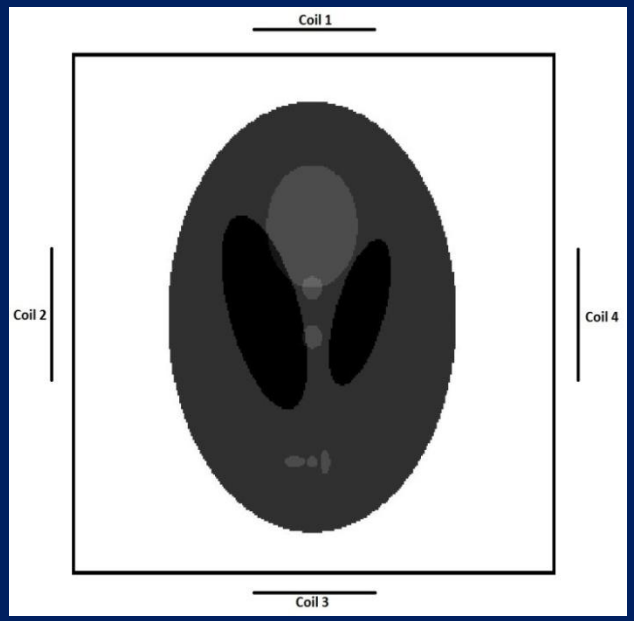
Image inverse Fourier Reconstruction for single coil.

$$(\Omega_{yR} + i\Omega_{yI}) * (F_R + iF_I) * (\Omega_{xR} + i\Omega_{xI})^T = (V_R + iV_I)$$



Bruce and Rowe: In progress.

Rowe, Marquette U



Background

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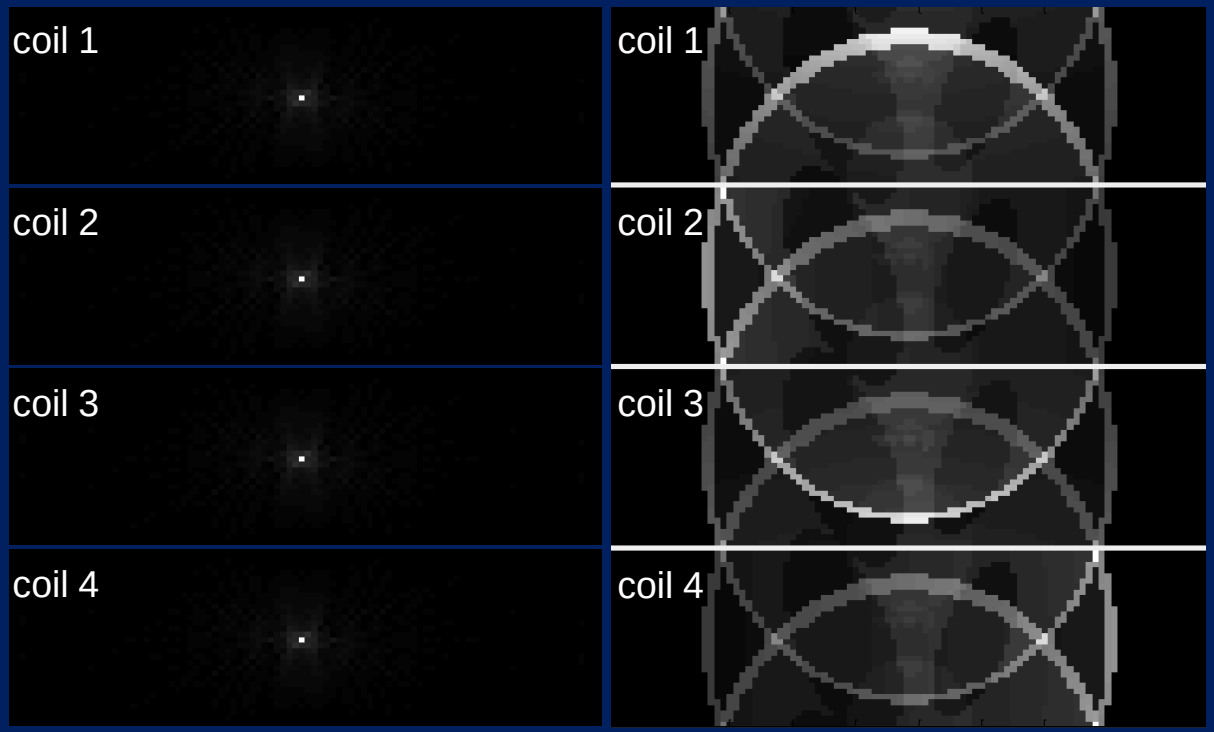
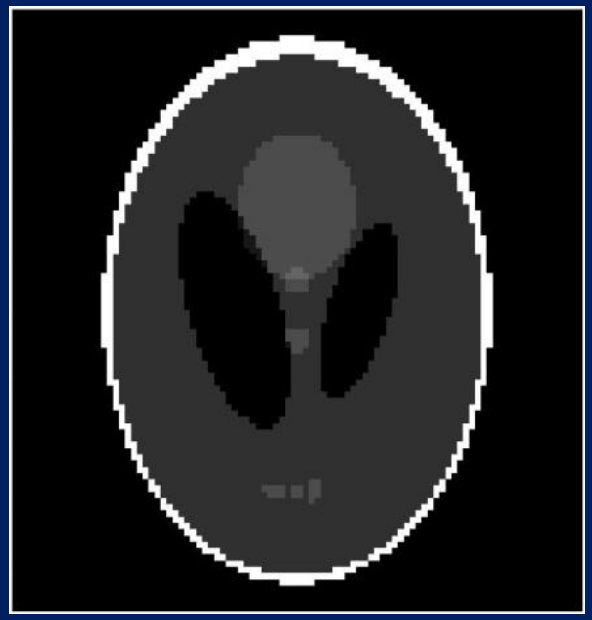
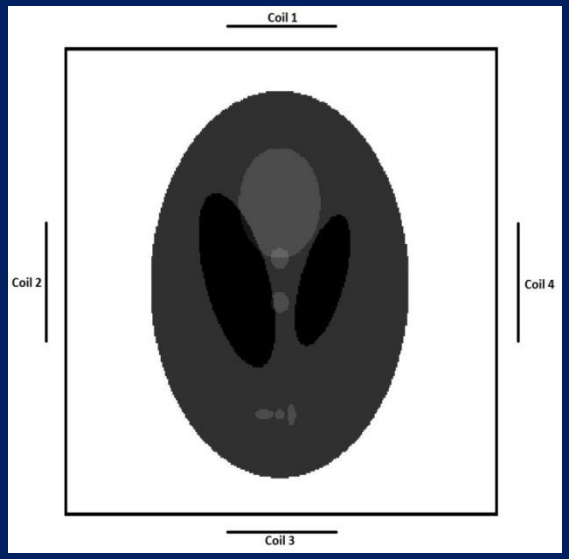




Bruce and Rowe: In progress.

Rowe, Marquette U



Background

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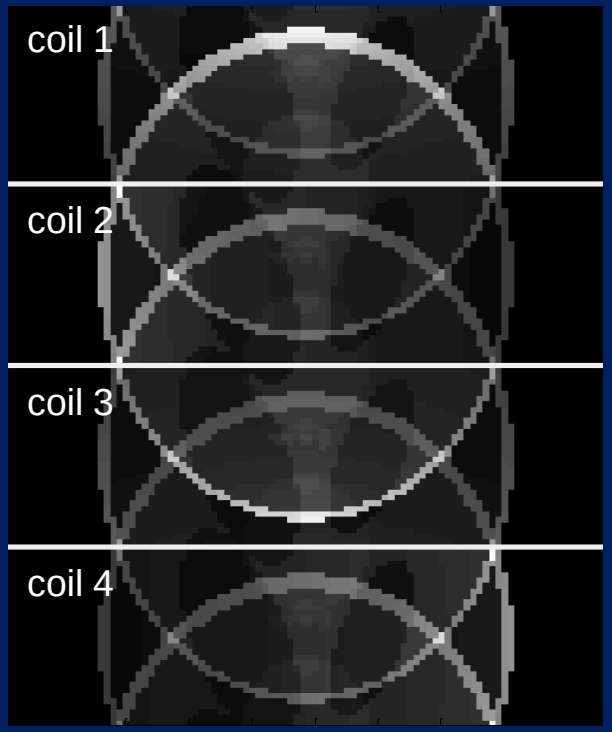
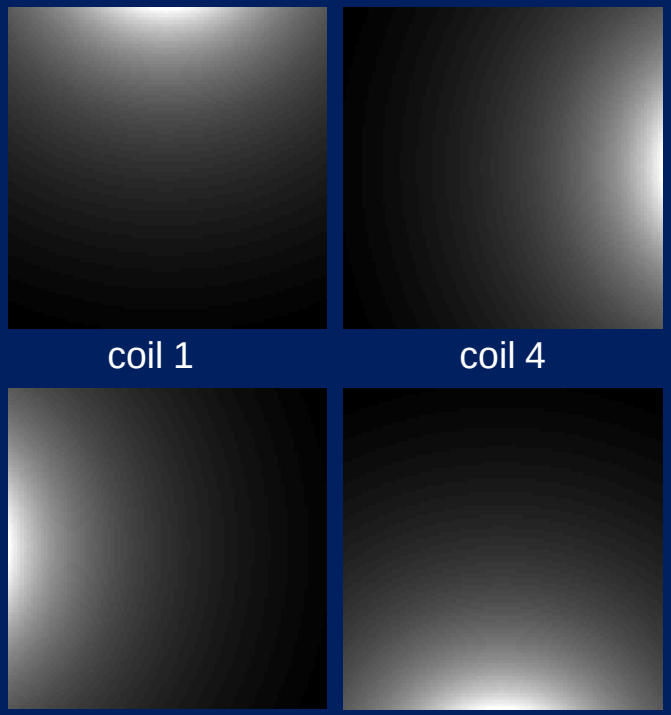


a_C



S_C

v_C

Bruce and Rowe: In progress.

Methods

The SENSE model for aliased voxel values from n coils is

$$\underset{n\times 1}{a_C} = \underset{n\times A}{S_C}\ \underset{A\times 1}{v_C} + \underset{n\times 1}{\varepsilon_C}\ , \quad \varepsilon_C \sim CN(0, \Psi_C)$$

where for each voxel $\Psi_C = \Psi_R + i\Psi_I$

a_C is a vector of the n complex-valued aliased voxel values

$a_C = a_R + ia_I$

v_C is a vector of the A unaliased voxel values

$v_C = v_R + iv_I$

S_C is an nxA matrix of complex-valued coil sensitivities

$S_C = S_R + iS_I$

ε_C is a vector of the n complex-valued error values

$\varepsilon_C = \varepsilon_R + i\varepsilon_I$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.

Methods

The SENSE process

$$\underset{n\times 1}{a_C} = \underset{n\times A}{S_C}\ \underset{A\times 1}{v_C} + \underset{n\times 1}{\varepsilon_C}, \quad \varepsilon_C \sim CN(0,\Psi_C)$$

$$\Psi_C = \Psi_R + i\Psi_I$$

uses the complex normal distribution

$$f(\varepsilon_C) = (2\pi)^{-n}\left|\Psi_C\right|^{-1} e^{-1/2\,\varepsilon_C^H \Psi_C^{-1}\varepsilon_C},$$

H is the conjugate transpose (Hermetian)

and for N_C coil measurements

$$f(a_C) = (2\pi)^{-n}\left|\Psi_C\right|^{-1} e^{-1/2(a_C - S_C v_C)^H \Psi_C^{-1}(a_C - S_C v_C)}$$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.
Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956.
Bruce and Rowe: In progress.

Methods

From the distribution for the n coil measurements

$$f(a_C) = (2\pi)^{-n} \left|\Psi_C\right|^{-1} e^{-1/2(a_C - S_C v_C)^H \Psi_C^{-1}(a_C - S_C v_C)}$$

the voxel values can be estimated as

$$v_C = (S_C^H \Psi_C^{-1} S_C)^{-1} S_C^H \Psi_C^{-1} a_C$$

with knowledge of S_C and Ψ_C.

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.
Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956.
Bruce and Rowe: In progress.

Methods

Instead of writing the model with complex numbers as

$$\underset{n\times 1}{a_C} = \underset{n\times A}{S_C}\ \underset{A\times 1}{v_C} + \underset{n\times 1}{\varepsilon_C},$$

$$a_C = a_R + ia_I \quad S_C = S_R + iS_I \quad v_C = v_R + iv_I \quad \varepsilon_C = \varepsilon_R + i\varepsilon_I$$

we can write the model using an isomorphism as

$$\underset{2n\times 1}{a} = \underset{2n\times 2A}{S}\ \underset{2A\times 1}{v} + \underset{2n\times 1}{\varepsilon}$$

$$a = \begin{pmatrix} a_R \\ a_I \end{pmatrix} \quad S = \begin{pmatrix} S_R & -S_I \\ S_I & S_R \end{pmatrix} \quad v = \begin{pmatrix} v_R \\ v_I \end{pmatrix} \quad \varepsilon = \begin{pmatrix} \varepsilon_R \\ \varepsilon_I \end{pmatrix}$$

Pruessmann et al.: SENSE: Sensitivity Encoding for Fast MRI. MRM 42:952–962, 1999.
Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956.
Bruce and Rowe: In progress.

Methods

Then the distribution for n coil measurements is

$$f(a) = (2\pi)^{-n} \left|\Psi_{SE}\right|^{-1/2} \mathrm{e}^{-1/2(a-Sv)'\Psi_{SE}^{-1}(a-Sv)},$$

with

$$a = \begin{pmatrix} a_R \\ a_I \end{pmatrix} \qquad S = \begin{pmatrix} S_R & -S_I \\ S_I & S_R \end{pmatrix} \quad v = \begin{pmatrix} v_R \\ v_I \end{pmatrix} \qquad \varepsilon = \begin{pmatrix} \varepsilon_R \\ \varepsilon_I \end{pmatrix}$$

and the complex normal distribution imposes skew-symmetric

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix}$$

Wooding The multivariate distribution of complex normal variables. Biometrika 43:212–215, 1956.
Bruce and Rowe: In progress.

Methods

The skew-symmetric covariance structure

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix}$$ is incorrect.

What this says is that $\mathrm{cov}(I, I) = \mathrm{cov}(R, R)$

and that $\mathrm{cov}(I, R) = -\mathrm{cov}(R, I)$.

The proper covariance structure should be

$$\Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix}$$

(SE for SENSE and SI for new covariance model SENSE-ITIVE)

Bruce and Rowe: In progress.

Methods

Examine the difference between the two covariance structures

$$\Psi_{SE} = \begin{pmatrix} \Psi_R & -\Psi_I \\ \Psi_I & \Psi_R \end{pmatrix} \qquad \Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix}$$

in the distribution

$$f(a) = (2\pi)^{-n} \left|\Psi_{SE/SI}\right|^{-1/2} \mathrm{e}^{-1/2(a-Sv)'\Psi_{SE/SI}^{-1}(a-Sv)}$$

through estimates

$$v_{SE} = (S'\Psi_{SE}^{-1}S)^{-1}S'\Psi_{SE}^{-1}a$$

$$v_{SI} = (S'\Psi_{SI}^{-1}S)^{-1}S'\Psi_{SI}^{-1}a$$

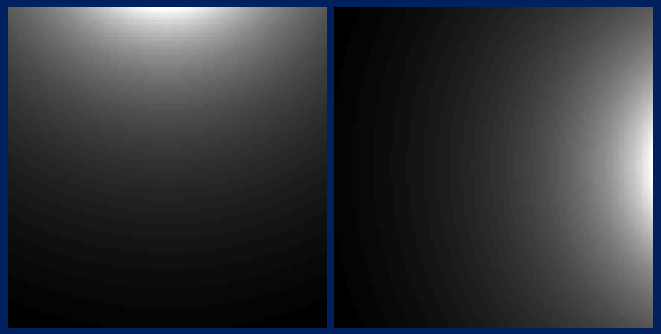
Bruce and Rowe: In progress.

Results

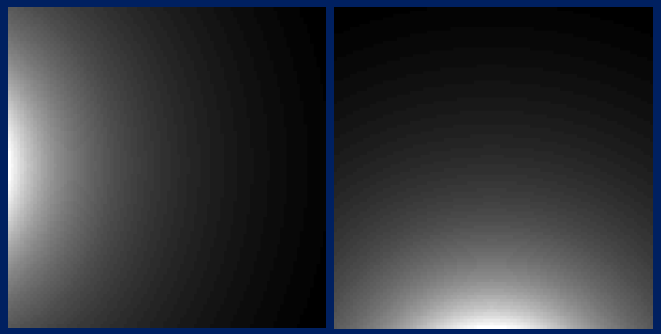
Noiseless multi-coil spatial frequency arrays are with

$$\Psi_{SI} = \begin{pmatrix} \Psi_R & \Psi_{RI} \\ \Psi'_{RI} & \Psi_I \end{pmatrix} \quad \Psi_R = \begin{pmatrix} 1 & .33 & .11 & .33 \\ .33 & 1 & .33 & .11 \\ .11 & .33 & 1 & .33 \\ .33 & .11 & .33 & 1 \end{pmatrix} \quad \Psi_{RI} = \begin{pmatrix} 0 & -.11 & -.07 & -.11 \\ .33 & 0 & -.11 & -.07 \\ .42 & .26 & 0 & -.11 \\ .26 & .42 & .26 & 0 \end{pmatrix}$$

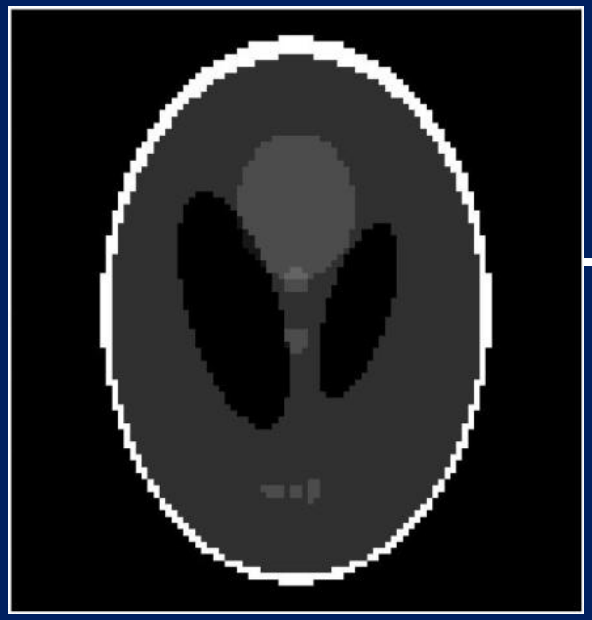
$$\Psi_I = \Psi_R$$

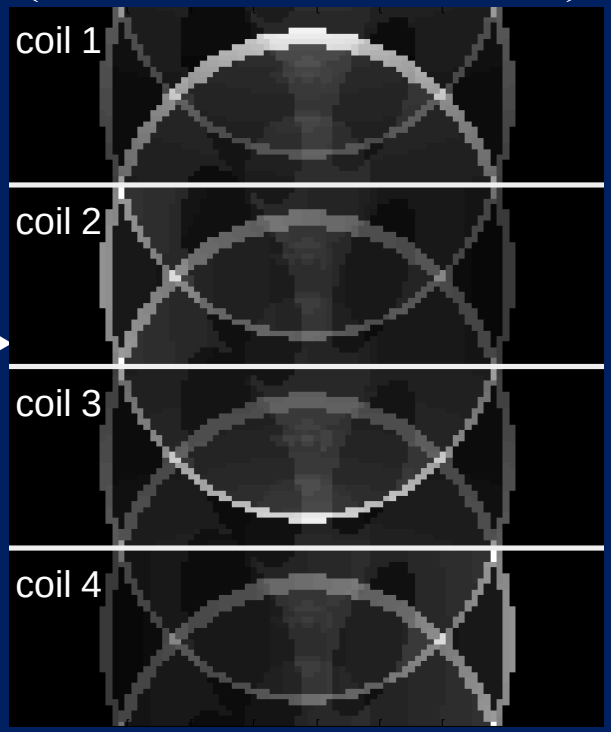


coil 1 coil 4



coil 2 coil 3





Bruce and Rowe: In progress.

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Results

Magnitude

SENSE

SENSE-ITIVE

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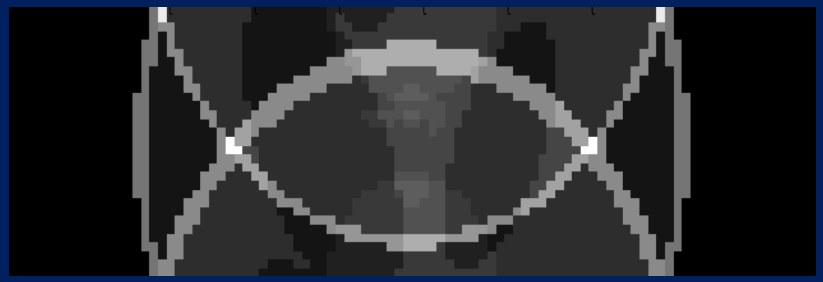
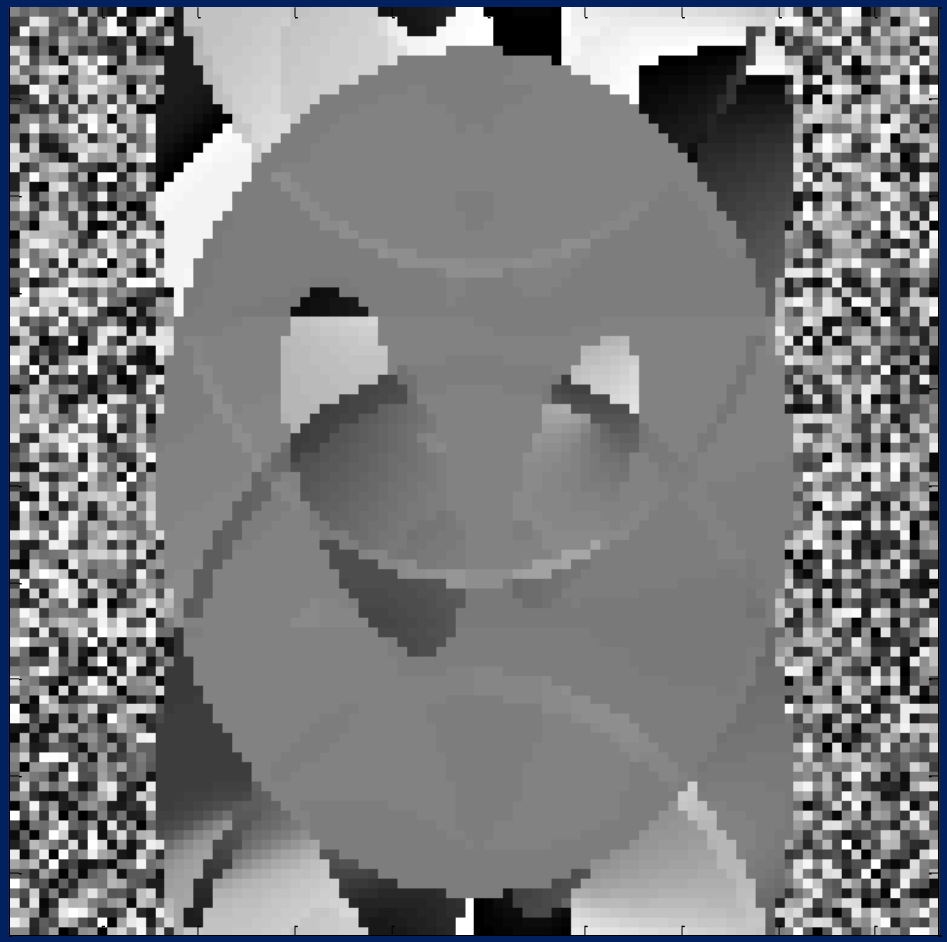
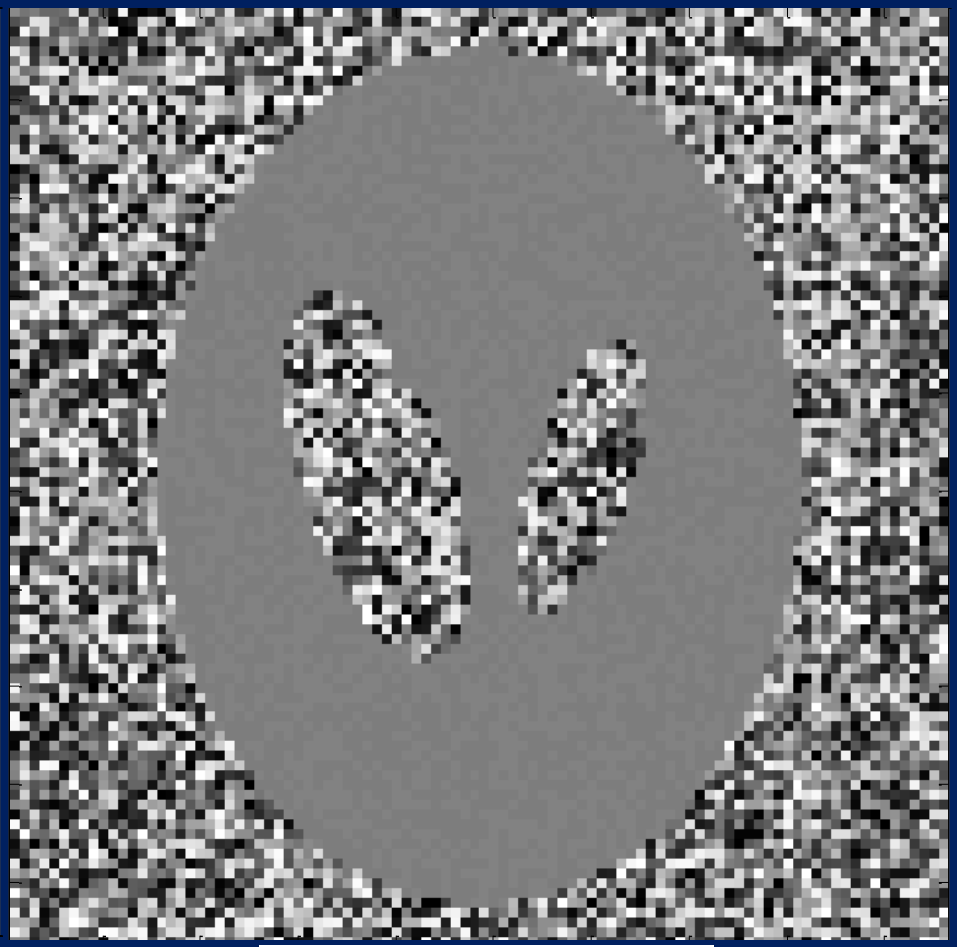


Results

Phase



SENSE



SENSE-ITIVE

Discussion

The SENSE image reconstruction method was described.

The SENSE reconstruction written with an isomorphism.

The covariance structure of complex SENSE described.

New SENSE-ITIVE method described with proper covariance.

Results of SENSE & SENSE-ITIVE reconstruction presented.

Ghosting present in SENSE magnitude and phase images.

Better reconstruction in SENSE-ITIVE reconstruction especially phase used for complex-valued time series activation.

Thank You

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Iain Bruce, Marquette University
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