

## Processing Induced Voxel Correlation in SENSE fMRI Via the AMMUST Framework

Daniel B. Rowe<sup>1,2</sup> and Iain P. Bruce<sup>1</sup>

<sup>1</sup>Department of Math, Stat, and Comp Sci, Marquette University, Milwaukee, Wisconsin, USA

<sup>2</sup>Department of Biophysics, Medical College of Wisconsin, Milwaukee, Wisconsin, USA

### Introduction:

It is well known that magnetic field gradients can be used to Fourier encode the complex-valued spatial frequencies of an object. From a two dimensional array of the complex-valued spatial frequencies for an object  $S_C$ , a complex-valued image  $V_C$  can be reconstructed via inverse Fourier transform as

$$V_C = \begin{matrix} \Omega_{C_y} & S_C & \Omega'_{C_x} \\ n_y \times n_x & n_y \times n_y & n_x \times n_x \end{matrix} \quad (1)$$

where  $\Omega_{C_x}$  and  $\Omega_{C_y}$  are complex-valued Fourier transform matrices. This reconstruction process is nearly always modified with image adjustments and preprocessing to reconstruct complex-valued images for subsequent (generally magnitude-only) statistical analysis. It has been shown that the two dimensional inverse Fourier transformation process in Equation 1 can be equivalently represented with a real-valued isomorphism representation [2]. This isomorphism representation stacks the real part of the rows of the array of spatial frequencies  $S_C$  upon the imaginary part of the rows of  $S_C$  to form a vector  $s$  that is pre-multiplied by an inverse Fourier transform reconstruction matrix  $\Omega$  to form a vector  $v$  of voxel values as

$$v = \begin{matrix} \Omega & s \\ 2n_x n_y \times 1 & 2n_x n_y \times 1 \end{matrix} \quad (2)$$

In Equation 2, both  $s$  and  $v$  contain real and imaginary measurements. This establishes a linear relationship between spatial frequencies and voxel values. With both preprocessing and reconstruction operations quantified as linear matrix operators, Equation 2 is generalized as

$$v = \begin{matrix} O_I & \Omega_a & O_k & s \\ 2n_x n_y \times 1 & 2n_x n_y \times 2n_x n_y & 2n_x n_y \times 2n_x n_y & 2n_x n_y \times 1 \end{matrix} \quad (3)$$

where  $O_k$  are potential operations in  $k$ -space,  $\Omega_a$  is an inverse Fourier transform matrix that can be adjusted for  $T_2^*$  and  $\Delta B_0$ , and  $O_I$  are potential image-space operations in the AMMUST framework [3]. It was shown that the covariance matrix  $\Sigma$  of the reconstructed voxels can be represented as

$$\Sigma = O_I \Omega_a O_k \Gamma O'_k \Omega'_a O'_I \quad (4)$$

where  $\Gamma$  is the covariance matrix for the spatial frequencies [3]. From Equation 4, a correlation matrix can be formed. With uncorrelated spatial frequencies in Equation 4,  $\Gamma=I$ , it was shown that preprocessing and reconstruction operations can induce spatial correlation between voxels [3].

### Methods:

The model in Equation 3 can be generalized to include the voxelwise SENSE multi coil image reconstruction method  $v_c = (S_C^H \Psi_C^{-1} S_C)^{-1} S_C^H \Psi_C^{-1} a_c$

where in a given voxel,  $S_C$  is the complex-valued coil sensitivity,  $H$  denotes the transposed complex conjugate,  $\Psi_C$  is the complex-valued noise covariance matrix [5], and  $a_c$  is the vector of complex-valued aliased voxel measurements [4]. This generalization is

$$v = O_I P_2 \begin{pmatrix} u_1 & \cdots & 0 \\ \vdots & \ddots & \vdots \\ 0 & \cdots & u_p \end{pmatrix} P_1 \begin{pmatrix} O_{I1} \Omega_{a1} O_{k1} & \cdots & 0 \\ \vdots & \ddots & \vdots \\ 0 & \cdots & O_{I1} \Omega_{an_c} O_{kn_c} \end{pmatrix} \begin{pmatrix} s_1 \\ \vdots \\ s_{n_c} \end{pmatrix}, \quad (5)$$

where  $n_c$  denotes the number of coils,  $s_j$  the aliased spatial frequency vector for coil  $j$ ,  $O_{kj}$  the operations on aliased spatial frequency vector for coil  $j$ ,  $\Omega_{aj}$  the adjusted reconstruction operator for aliased spatial frequency vector for coil  $j$ ,  $O_{Ij}$  the image space operations on the reconstructed image vector from the aliased spatial frequency vector for coil  $j$ ,  $P_1$  is a permutation that reorders values from by coil image to by voxel,  $u_q$  denotes an isomorphism matrix representation for a SENSE reconstruction of voxel  $q$ ,  $p$  is the total number of voxels,  $P_2$  is a permutation that reorders values from by unaliased voxel to unaliased image, and  $O_I$  are the image space operations on the combined reconstructed image vector. If Equation 5 is written as  $v=Os$ , then the covariance between voxels is  $\Sigma=OO'$ , with an identity spatial frequency correlation. The correlation matrix  $R$  can be found.

### Results and Discussion:

A true noiseless vector of  $n_c=4$  aliased image spatial frequencies was generated for a  $48 \times 48$  image with a reduction factor of 3. The coil covariance matrix is  $\text{real}(\Psi_C) = \text{imag}(\Psi_C) = [1, \rho, \rho^2, \rho; \rho, 1, \rho, \rho^2; \rho^2, \rho, 1, \rho; \rho, \rho^2, \rho, 1]$  where  $\rho=0.33$ . In reconstruction,  $O_{kj}$  included apodization of each image with a FWHM=2 voxels,  $\Omega_{aj}=\Omega$ ,  $u_j$  contains the true sensitivity and coil covariance matrix, while  $O_I=I$ . An image of the induced correlation for magnitude squared data (which is asymptotically equivalent to magnitude data) from preprocessing for the center voxel is presented in Figure 1 superimposed upon the reconstructed mean image. It is readily apparent that there is induced local correlation from apodization and induced correlation of the center voxel of interest with two others regions from the SENSE unfolding procedure.

### Conclusions:

Previous work that theoretically describes induced correlation between image voxels from spatial preprocessing and reconstruction operations has been summarized [3]. This previous work has been extended to include the SENSE multi coil image reconstruction method [4]. This has null hypothesis fMRI connectivity implications as the no connectivity scenario is not for no spatial correlation but is rather for the spatial correlation induced by preprocessing.

### References:

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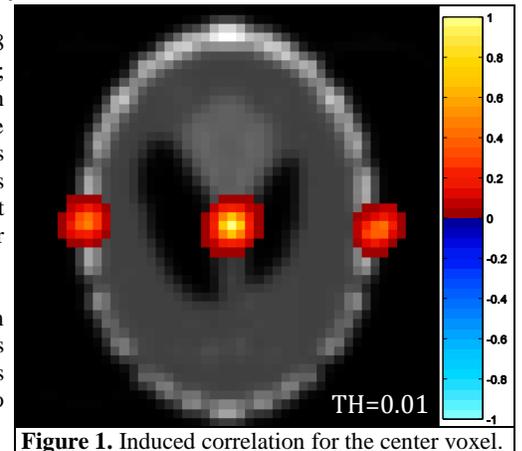


Figure 1. Induced correlation for the center voxel.